

The Eurasia Proceedings of Science, Technology, Engineering & Mathematics (EPSTEM), 2023

Volume 25, Pages 134-149

ICBAST 2023: International Conference on Basic Sciences and Technology

Numerical Computation of NMR Magnetization for Various Tissues in the Human Body Using Oringinpro

Bilyaminu Usman

Zamfara State College of Education

Ahmed Jimoh

Kebbi State University of Science and Technology

Abstract: Nuclear magnetic resonance (NMR) spectroscopy and imaging are arguably the most versatile techniques use in biomedical research today. NMR spectroscopy is a powerful and theoretical analytical tools. Since the development of NMR spectroscopy it is has become a very important tools in the field of medicine because of it being safer than the X-ray crystallography which has radiation effects on the human body. The most attractive features of NMR techniques are the wide range of biological processes that can be investigated using these methods and the variety and versatility of the specific MR techniques that can be applied. diagnosis of diseases. With the advent of computer programme, different computer programme has also being developed for NMR spectroscopy for performing different analysis on how electromagnetic radiation interact with various form of matter. This research perform NMR analysis of different tissue in the human body using Originpro. The research investigates various tissues of the human body, with the aid of Bloch flow equation the research obtained the transverse magnetization equation that was used for the tranverse magnetization map for the different tissues. Three different relaxation times consider for the different biological tissues are 0.5 T, 1.0 T and 1.5 T. The transverse magnetization for the various tissues are calculated at different magnetic flux density, at range of 0-0.02 seconds and a length for the tissues were in the range of 4.5×10^{-12} to 4.5×10^{-5} m. The result shows that transverse magnetization was greater at 0.5 T for the tissues considered at the range of 4.5×10^{-12} to 4.5×10^{-5} m.

Keywords: Bloch Equation, NMR, Relaxation time, Tissues, OriginPro

Introduction

Nuclear magnetic resonance which is commonly abbreviated as NMR by scientists is a physical phenomenon when the nucleus of certain atoms is immersed in a static magnetic field and exposed to another oscillating magnetic field. NMR also refers to a physical principle response of nuclei to a magnetic field (Grover et al., 2015). Many nuclei possess magnetic moment, they act like spinning bar magnets. These spinning bar magnetic nuclei interact with externally applied magnetic fields, producing measurable signals (Levitt, 2013).

The phenomenon of NMR has been known since 1946 and is widely used as an analytical tool in physics and chemistry (Reid et al., 1982). At approximately the same time, it was demonstrated that the use of magnetic field gradients could be used to encode NMR signals spatially (Cooley et al., 2015), and thus the concept of magnetic resonance imaging (MRI) was born. Soon thereafter, MR images of the human body were obtained and as early as 1980, the evaluation of MRI as a clinically useful imaging modality had started (Mammarappallil et al., 2019).

- This is an Open Access article distributed under the terms of the Creative Commons Attribution-Noncommercial 4.0 Unported License, permitting all non-commercial use, distribution, and reproduction in any medium, provided the original work is properly cited.

- Selection and peer-review under responsibility of the Organizing Committee of the Conference

© 2023 Published by ISRES Publishing: www.isres.org

Spectroscopy is the study of how electromagnetic radiation such as gamma rays, alpha, x-ray and other electromagnetic radiation interacts with matter (Farrukh, 2012). There are various method of spectroscopy such as Raman spectroscopy, X-ray spectroscopy, NMR spectroscopy etc. Nuclear magnetic resonance (NMR) spectroscopy and imaging are arguably the most versatile techniques use in biomedical research today. NMR spectroscopy is used to study the behavior of matter such as the physical, chemical and biological properties of matter (Albrecht et al., 2015). For the past six decades NMR spectroscopy has become the most significance of all the method of spectroscopy for determining the structure of organic compounds. NMR spectroscopy is a powerful and theoretical analytical tool.

NMR spectroscopy finds applications in several areas of science. NMR spectroscopy is routinely used by chemists to study chemical structure using simple one-dimensional techniques. The use of NMR to study the structure of proteins and other biological molecules was markedly improved in the late 1960s with the development of superconducting magnets and the implementation of Fourier transform NMR (Moser et al., 2017). However, it was not until the mid-1970s that the first applications of NMR to the study of metabolism in living biological systems were reported (Becker, 1993). Two-dimensional techniques are used to determine the structure of more complicated molecules. These techniques are replacing x-ray crystallography for the determination of protein structure (Ginsberg et al., 2009).

NMR spectroscopy is widely employed in the analysis of properties of matter. It is also employed in checking defects in finished products in industry (Lovchinsky et al., 2016), it is also used by the chemist in studying the molecular structure of chemical compound, in medicine NMR spectroscopy is used in determining diseases in the human tissues such as skeletal tissue, liver, fatty tissues and other tissues (Seabolt et al., 2015).

Since the development of NMR spectroscopy it is has become a very important tools in the field of medicine because of it being safer than the X-ray crystallography which has radiation effects on the human body. The most attractive features of NMR techniques are the wide range of biological processes that can be investigated using these methods and the variety and versatility of the specific MR techniques that can be applied. For example, it is possible to study glucose metabolism in isolated neuronal cells in culture, in vivo in the brain of an animal, and in humans using the same basic techniques (Nagy & Einwallner, 2018).

Apart from NMR spectroscopy there is also Nuclear Magnetic Resonance Imaging which is also abbreviated as MRI. MRI is an imaging technique used in medicine for investigating the physiology and anatomy of the human body for health and disease (Giza et al., 2021). The instrument used for MRI is called MRI scanner which make use of radio waves and magnetic fields to produce the images of the human body. This technique is used in health centres for diagnosis of diseases. With the advent of computer programme, different computer programme has also being developed for NMR spectroscopy for performing different analysis on how electromagnetic radiation interact with various form of matter (Miller et al., 2014).

Performing Nuclear Magnetic Resonance (NMR) data analysis and processing of Nuclear magnetic resonance spectral require the use of NMR instrument such as the nuclear magnetic resonance spectrometer. These instruments are very expensive and the cost of maintenance is high. In order for us to easily access the use of NMR spectroscopy, a computer programme that can simulate NMR can be used. The ability to able to use computer programme to perform analysis and processing of NMR data will make it easy and also readily available to investigate the property of matter. This research used origin 9.0 for processing and analysing NMR data. The aim of this research is to perform NMR analysis of different tissue in the human body using Originpro. In other to achieved the aim the research will obtained the transverse magnetization equation from NMR Bloch flow equation and present a graph of transverse magnetization map for each of the tissues in the human body.

Methodology

Bloch Flow Equations

The NMR Bloch flow equations for bulk protons moving at a variable velocity $v(x)$ is given as;

$$v^2(x) \frac{d^2 M_y}{dx^2} + v(x)(T_0 + \frac{dv}{dx}) \frac{dM_y}{dx} + (\gamma^2 B_1^2(x) + T_g) M_y = \frac{M_0}{T_1} \gamma B_1(x) \quad (1)$$

(Awojoyegbe et al., 2011)

If the Radio Frequency field $B_1(x)$ is applied such that M_y is sampled at maximum magnitude, then $M_0 \approx 0$ equation (1) becomes;

$$v^2(x) \frac{d^2 M_y}{dx^2} + v(x)(T_0 + \frac{dv}{dx}) \frac{dM_y}{dx} + (\gamma^2 B_1^2(x) + T_g) M_y = 0 \quad (2)$$

$$T_0 = \frac{1}{T_1} + \frac{1}{T_2}, \quad T_g = \frac{1}{T_1 T_2} \quad (3)$$

Assuming that the fluid velocity and the applied field have the forms;

$$v(x) = \frac{x}{\delta} \quad \text{And} \quad B_1(x) = \frac{T_g}{T_0^2} G(x) \quad (4)$$

From Equation (4) we have that $v(x) = \frac{x}{\delta}$, differentiating with respect to the variable x

$$\begin{aligned} \frac{dv}{dx} &= \frac{d\left(\frac{x}{\delta}\right)}{dx} \\ \frac{dv}{dx} &= \frac{1}{\delta} \end{aligned} \quad (5)$$

Substitute equation (4) and (5) into (3), we have that

$$\frac{x^2}{\delta^2} \frac{d^2 M_y}{dx^2} + \frac{x}{\delta} (T_0 + \frac{1}{\delta}) \frac{dM_y}{dx} + (\frac{T_g^2}{T_0^4} \gamma^2 G^2 x^2 + T_g) M_y = 0 \quad (6)$$

Multiply equation (6) by δ^2

$$\begin{aligned} \delta^2 \left[\frac{x^2}{\delta^2} \frac{d^2 M_y}{dx^2} + \frac{x}{\delta} (T_0 + \frac{1}{\delta}) \frac{dM_y}{dx} + (\frac{T_g^2}{T_0^4} \gamma^2 G^2 x^2 + T_g) M_y \right] &= 0 \\ x^2 \frac{d^2 M_y}{dx^2} + x \delta (T_0 + \frac{1}{\delta}) \frac{dM_y}{dx} + \delta^2 (\frac{T_g^2}{T_0^4} \gamma^2 G^2 x^2 + T_g) M_y &= 0 \\ x^2 \frac{d^2 M_y}{dx^2} + x (\delta T_0 + 1) \frac{dM_y}{dx} + (\frac{T_g^2}{T_0^4} \gamma^2 G^2 \delta^2 x^2 + \delta^2 T_g) M_y &= 0 \end{aligned} \quad (7)$$

$$\text{Set } \xi = \frac{T_g}{T_0^2} \gamma G \delta \quad (8)$$

Put equation (7) into (6)

$$x^2 \frac{d^2 M_y}{dx^2} + x(1 + \delta T_0) \frac{dM_y}{dx} + (\xi^2 x^2 + \delta^2 T_g) M_y = 0 \quad (9)$$

Equation (9) is a form of Besse1 differential equation, which has a genera1 equation as;

$$x^2 \frac{d^2 y}{dx^2} + x(2p + 1) \frac{dy}{dx} + (a^2 x^{2r} + \beta^2) y = 0 \quad (10)$$

Equation (10) has a genera1 solution as;

$$y = x^{-p} \left[c_1 J_{q/r} \left(\frac{a}{r} x^r \right) + c_2 Y_{q/r} \left(\frac{a}{r} x^r \right) \right] \quad (11a)$$

Where,

$$q = \sqrt{p^2 + \beta^2} \quad (11b)$$

Comparing equation (9) and (10) gives;

$$\begin{aligned} y &= M_y & r &= 1 & a &= \xi \\ 2p &= \delta T_0 & \beta^2 &= \delta^2 T_g \end{aligned} \quad (12)$$

From equation (12);

$$\begin{aligned} 2p &= \delta T_0 \\ p &= \frac{\delta T_0}{2} \end{aligned} \quad (13)$$

Substituting equation (13) into equation (11)

$$\begin{aligned} q &= \sqrt{p^2 - \beta^2} \\ q &= \sqrt{\left(\frac{\delta T_0}{2} \right)^2 - \delta^2 T_g} \\ q &= \frac{\delta}{2} \sqrt{T_0^2 - 4T_g} \end{aligned} \quad (15)$$

Using the general solution in equation (11) to solve equation (9)

$$M_y(x) = x^{-\frac{\delta T_0}{2}} \left[c_1 J_{\frac{\delta}{2} \sqrt{T_0^2 - 4T_g}}(\xi x) + c_2 Y_{\frac{\delta}{2} \sqrt{T_0^2 - 4T_g}}(\xi x) \right] \quad (16)$$

Put $\alpha = -\frac{\delta T_0}{2}$ $n = \frac{\delta}{2} \sqrt{T_0^2 - 4T_g}$ in equation (16)

$$M_y(x) = x^\alpha [c_1 J_n(\xi x) + c_2 Y_n(\xi x)] \quad (17)$$

C_1 and C_2 are constants. Since it is required that the transverse magnetization be finite at all points, then the constant C_2 must be zero because the second kind Bessel's function (Y_n) tends to infinite at $x = 0$. Hence equation (17) will be reduced to;

$$M_y(x) = x^\alpha c_1 J_n(\xi x) \quad (18)$$

Equation (18) is the transverse magnetization derived from the NMR Bloch flow equation

Proton Relaxation Times for the Various Biological Tissue

Tissues in the human being are soft and these tissues fall in between the range of solids and pure fluids. In regards to relaxation property, the tissues can be treated as viscous fluids that is the fluid that resists to flow. The proton relaxation times for the different biological tissues of the human body which include liver, Fatty tissue, grey brain matter and white brain matter is shown Table 1 below. This table shows the proton relaxation times of the various biological tissues at 0.5T, 1.0T and 1.5T.

Table 1. Proton relaxation times of biological tissues (Bottomley *et al.* 1984).

Tissue	T_2 (ms)	T_1 (s) at 0.5T	T_1 (s) at 1.0T	T_1 (s) at 1.5T
Liver	53	0.44	0.48	0.56
Fatty tissue	90	0.26	0.2	0.29
Grey brain matter	110	0.7	0.75	0.97
White brain matter	102	0.63	0.7	0.71

Calculation of Transverse Magnetization

The transverse magnetization for the various tissues are calculated at different magnetic flux density, at range of 0-0.02 seconds for δ and the following ranges for the displacement in metre;

$$\begin{aligned}
 & \text{(i)} \quad x: 0 \text{ to } 4.5 \times 10^{-3} \\
 & \text{(ii)} \quad x: 0 \text{ to } 4.5 \times 10^{-6} \\
 & \text{(iii)} \quad x: 0 \text{ to } 4.5 \times 10^{-9} \\
 & \text{(iv)} \quad x: 0 \text{ to } 4.5 \times 10^{-12} \\
 & \text{And } G = 0.02, \quad \square = \frac{\square}{\square} \frac{6400000}{1.5} \square \text{ S}^{-1} \text{ T}^{-1}. \quad (19)
 \end{aligned}$$

Results and Discussion

From the tables of transverse magnetization that were obtained, OriginPro computer program was used to plot the transverse magnetization maps of liver, fatty tissues, grey brain matter and white brain matter for T_1 relaxation time at 0.5T, 1.0T and 1.5T. Putting into consideration the sample length at the various ranges. Comparative analysis was carried out on the transverse magnetizations maps for each tissue that we have. In order to do this, we put together tissues of the same sample length for the three different T_1 relaxation time at 0.5T, 1.0T and 1.5T. P1, P2 and P3 represent the T_1 relaxation time at 0.5T, 1.0T and 1.5T respectively. Figure 1 below is the transverse magnetization maps of the liver, we see that the magnetization of the plots P1 that is at 0.5T were greater than the magnetization obtained for 1.0T and 1.5T which is indicated by the red region, the high magnetization falls in between 10.93 and 15.00 ampere/meter for 0.5T, for 1.0T it falls between 10.61 and 1.90 ampere/meter and for 1.5T it falls between 9.23 and 13.10 ampere/meter. They are indicated on the map by the red region. Therefore, it will be sufficient enough to make use of T_1 relaxation at 0.5T for the magnetization at a sample length from 0 to 4m for the liver.

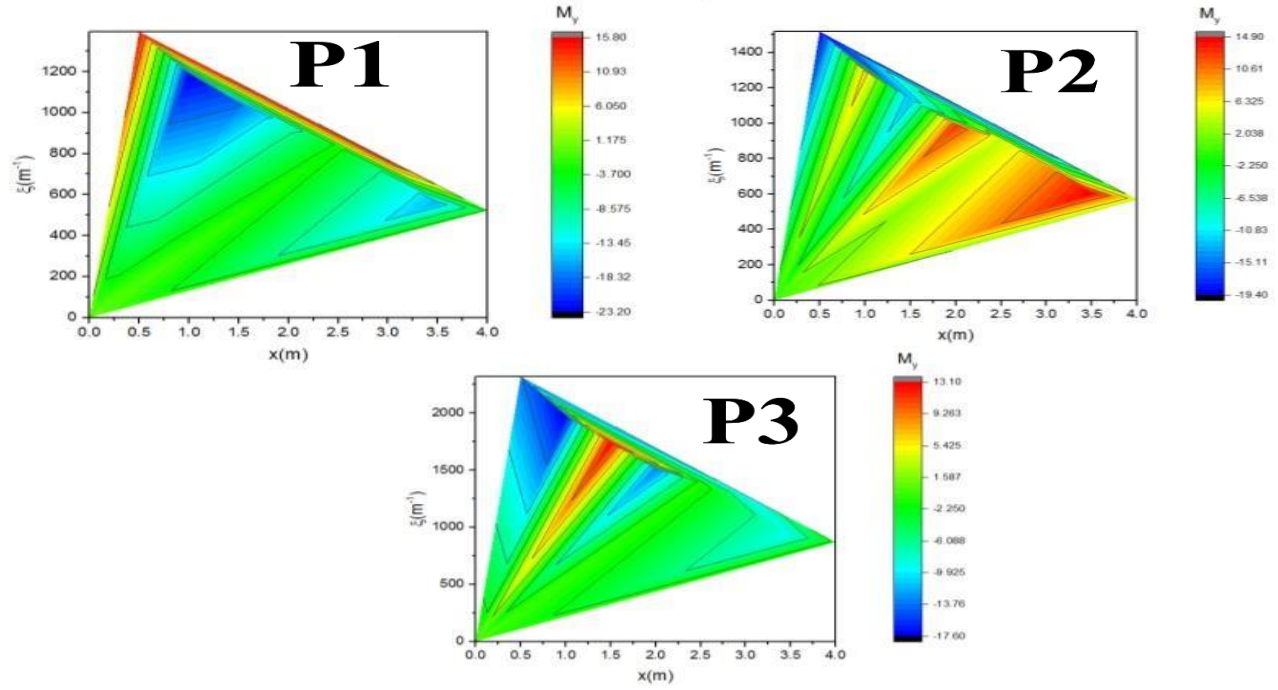


Figure 1. Transverse magnetization map for Liver in the Range of value of x: 0 to 4m

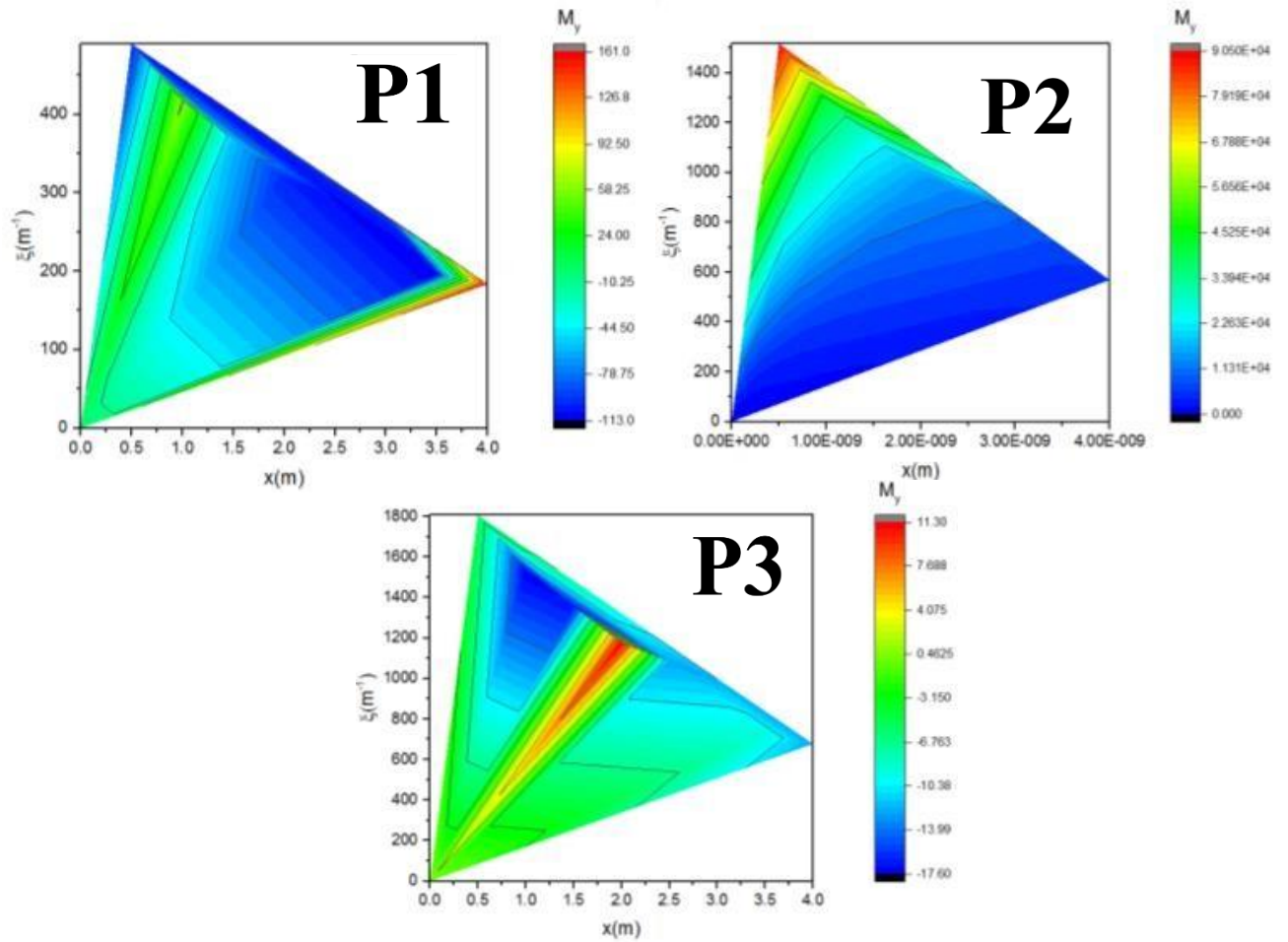


Figure 2. Transverse magnetization map for Fatty tissues in the Range of value of x: 0 to 4m

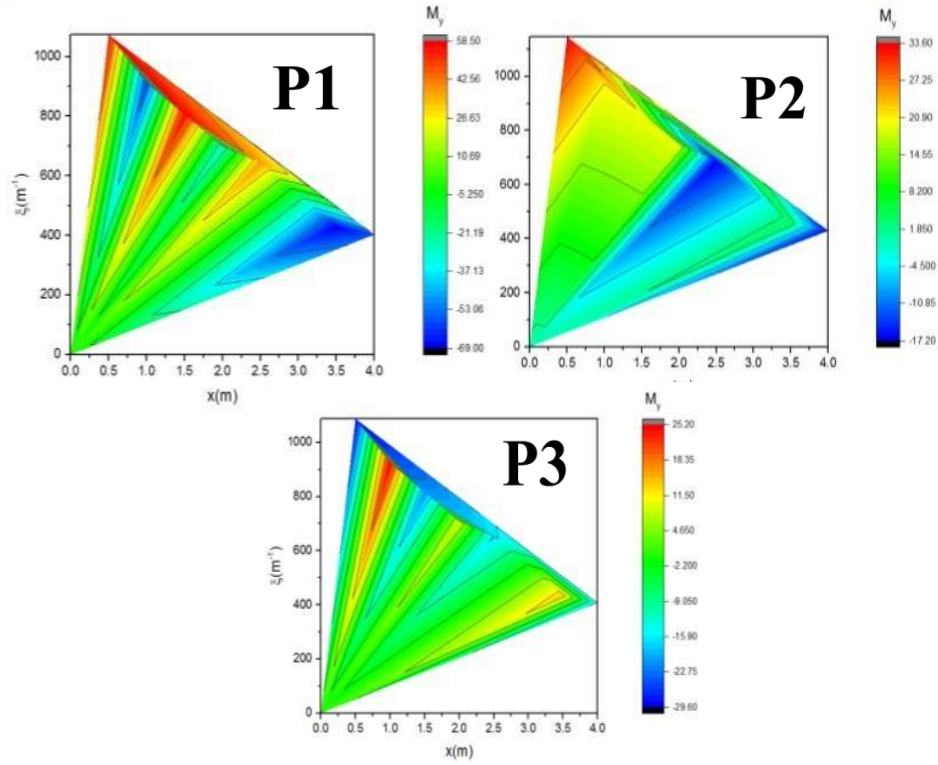


Figure 3. Transverse magnetization map for Grey brain matter in the Range of value of x : 0 to 4m

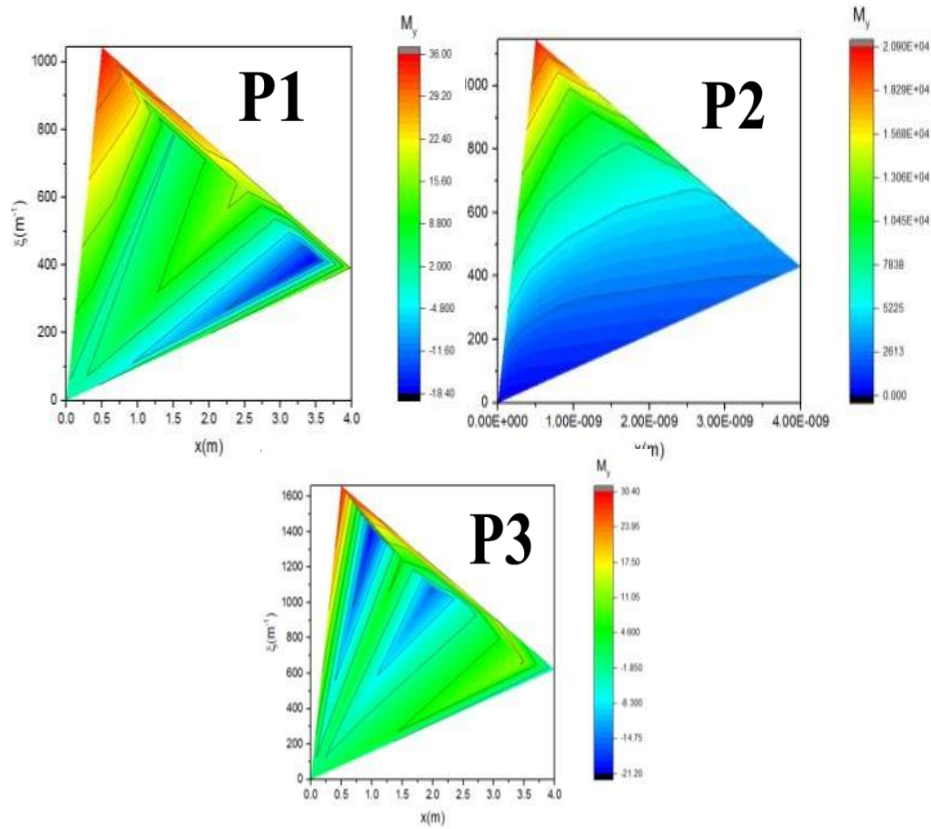


Figure 4. Transverse magnetization map for white brain matter in the Range of value of x : 0 to 4m

For the fatty tissues shown in figure 2, there is high magnetization between 126.8 and 161.0ampere/meter for 0.5T, for 1.0T it falls between 7.919×10^4 and 9.650×10^4 ampere/meter and for 1.5T it falls between 7.680 and 11.30ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 3.0 to 4.0m. Figure 3 is the transverse magnetization map for grey brain matter there is high magnetization between 42.56 and 58.50ampere/meter for 0.5T, for 1.0T it falls between 27.25 and 33.60ampere/meter and for 1.5T it falls between 18.35 and 25.20ampere/meter. They are indicated on the map by the red region. It will be best to make use of 0.5T for the magnetization at sample length between 0.1 to 2.0m. For the white brain matter shown in figure 4, there is high magnetization between 29.20 and 36.00ampere/meter for 0.5T, for 1.0T it falls between 1.829×10^4 and 2.90×10^4 ampere/meter and for 1.5T it falls between 23.95 and 30.40ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.1 to 3.0m

Figure 5 below compare the transverse magnetization maps of the liver, we see that the high magnetization falls in between 2.433×10^4 and 2.780×10^4 ampere/meter for 0.5T, for 1.0T it falls between 1.855×10^4 and 1.90ampere/meter and for 1.5T it falls between 6405 and 7320ampere/meter. They are indicated on the map by the red region. Therefore, it will be sufficient enough to make use of T_1 relaxation at 0.5T for the magnetization at a sample length from 0.000001 to 0.000004m for the liver. For the fatty tissues as shown in figure 6 there is high magnetization between 2325 and 5700ampere/meter for 0.5T, for 1.0T it falls between 1.260×10^6 and 1.440×10^6 ampere/meter and for 1.5T it falls between 3973 and 4540ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.0000005 to 0.0000015m.

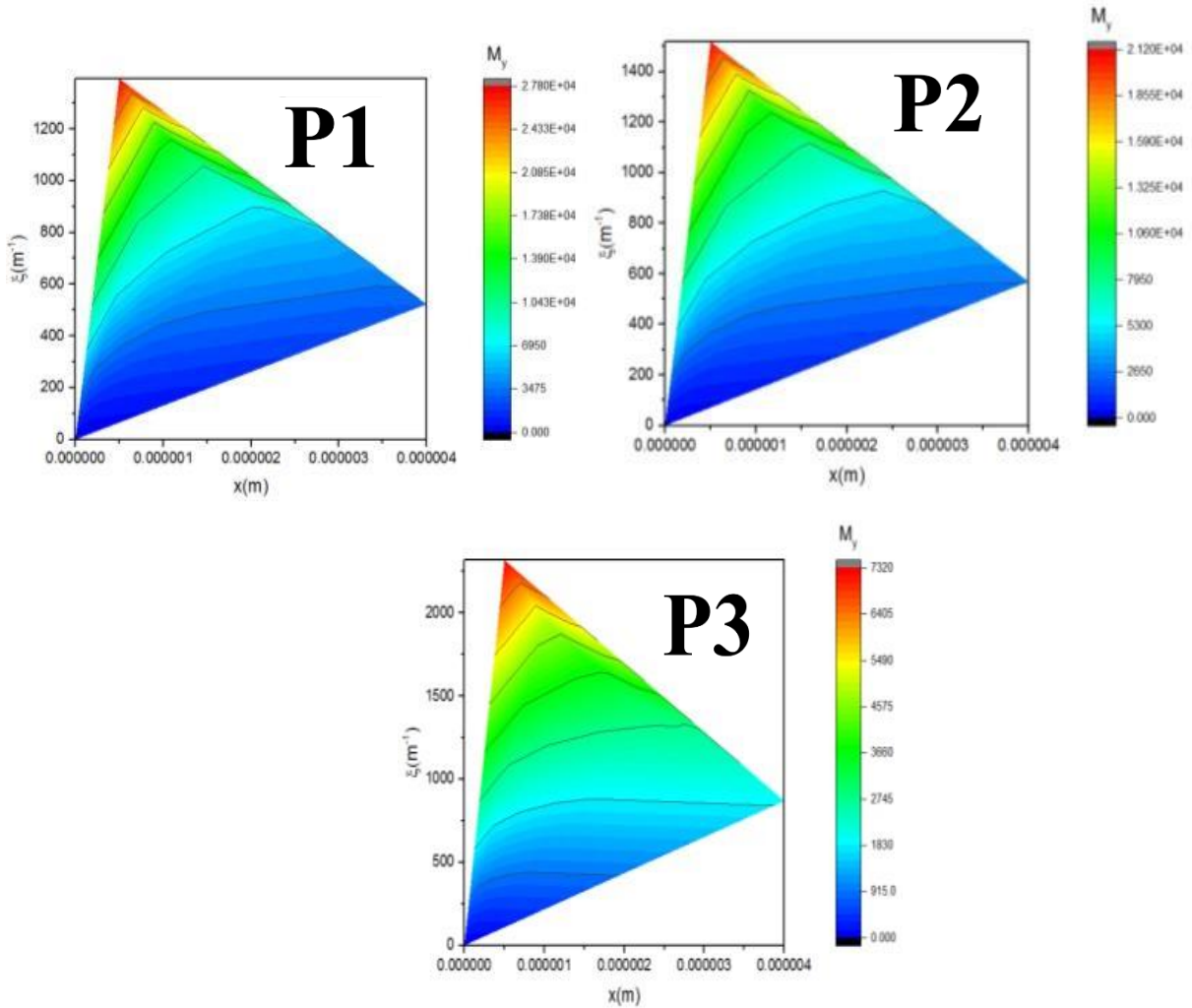


Figure 5. Transverse magnetization map for Liver in the Range of value of x: 0 to to 4×10^{-6} m

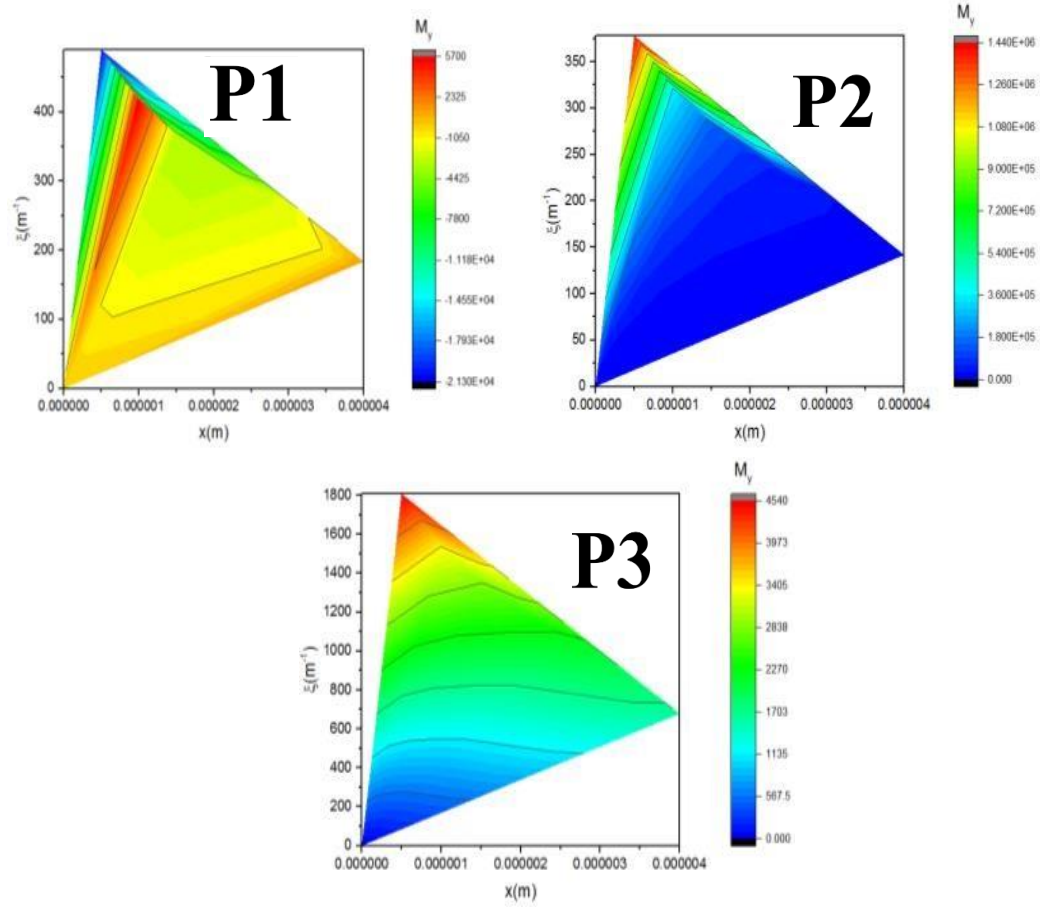


Figure 6. Transverse magnetization map for Fatty tissues in the Range of value of x: 0 to 4E-6 m

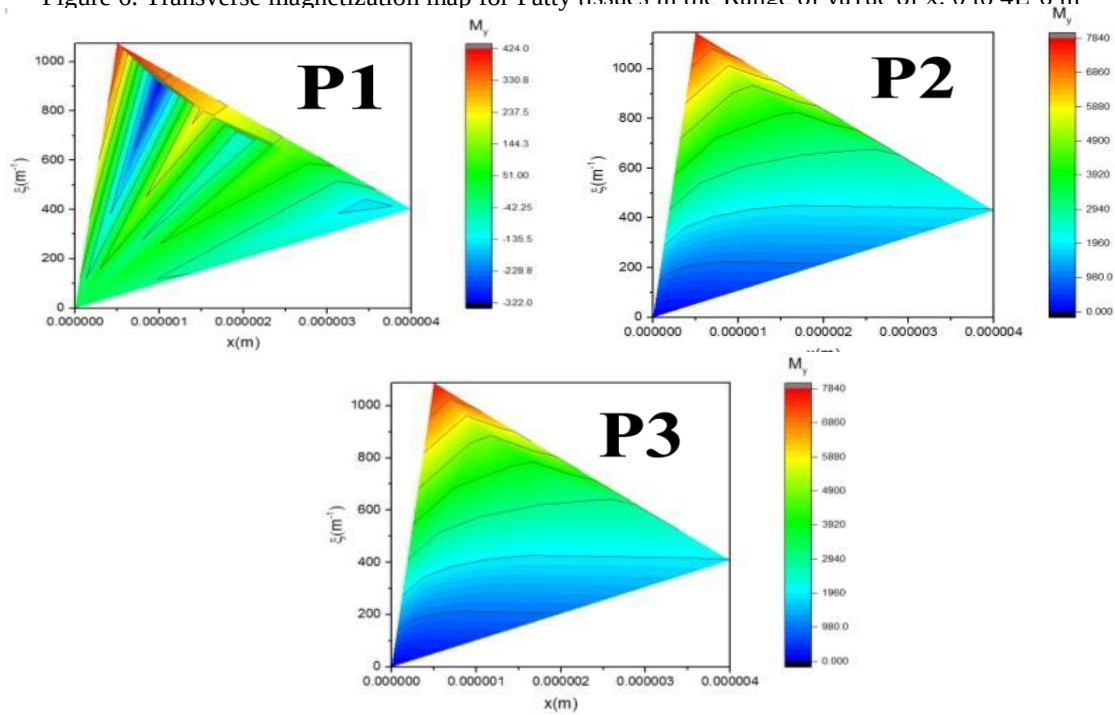


Figure 7. Transverse magnetization map for grey matter in the Range of value of x: 0 to 4E-6 m

Figure 7 is the magnetization for the grey brain matter there is high magnetization between 42.56 and 58.50ampere/meter for 0.5T, for 1.0T it falls between 27.25 and 33.60ampere/meter and for 1.5T it falls between 18.35 and 25.20ampere/meter. They are indicated on the map by the red region. It will be best to make use of 0.5T for the magnetization at sample length between 0.0000005 to 0.000002m.

For the white brain matter (figure 8), there is high magnetization between 29.20 and 36.00ampere/meter for 0.5T, for 1.0T it falls between 1.829E+4 and 2.90E+4ampere/meter and for 1.5T it falls between 23.95 and 30.40ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.0 to 0.0000015m.

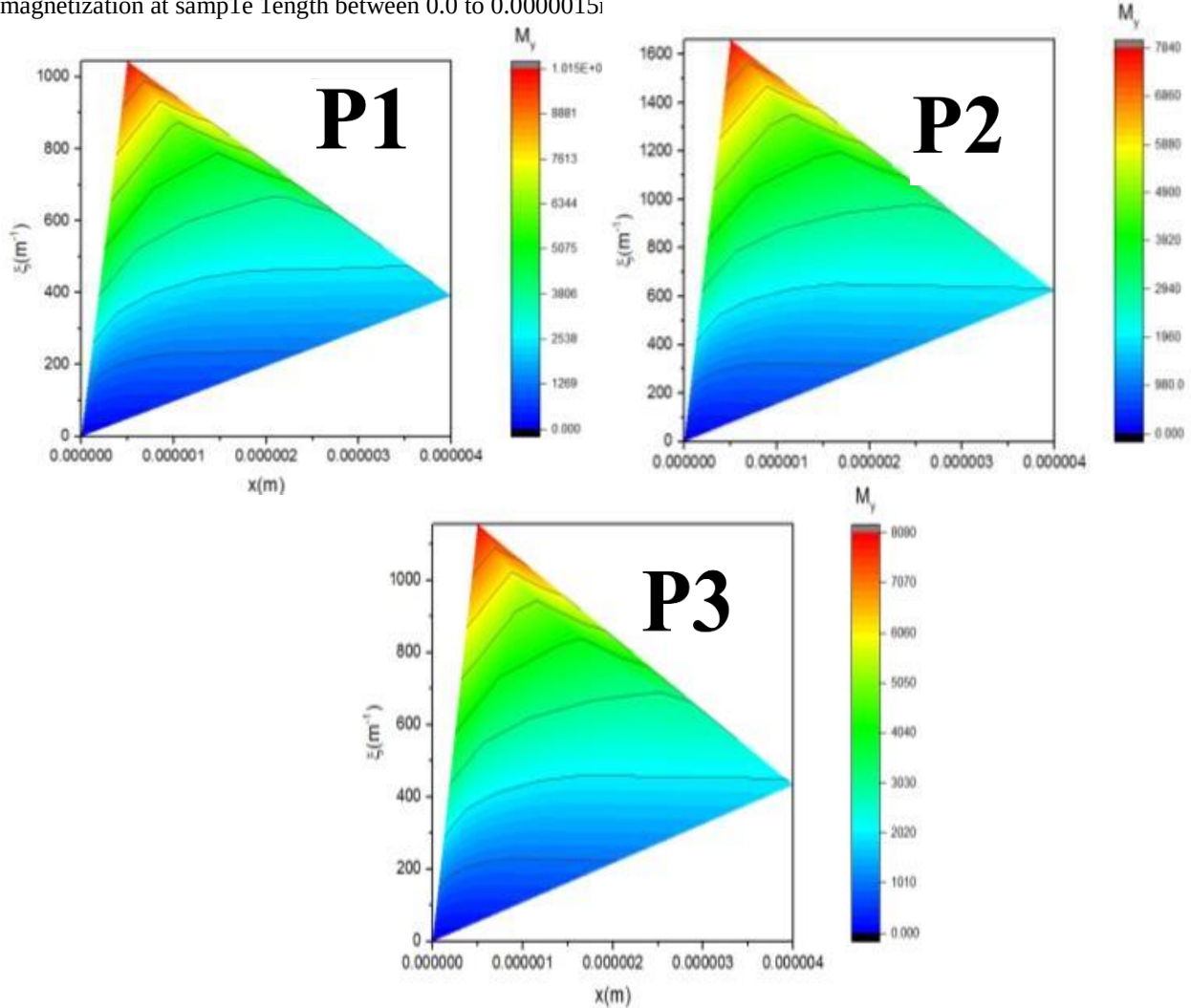


Figure 8. Magnetization map for White brain matter in the Range of value of x: 0 to 4E-6 m

Figure 9 below shows the transverse magnetization maps at sample length between 0 to 4E-9. For the liver, we see that the high magnetization falls in between .1186E+6 and 1.355E+6ampere/meter for 0.5T, for 1.0T it falls between 7.919E+4 and 9.050E+4ampere/meter and for 1.5T it falls between 1.649E+4 and 1.885+4ampere/meter. They are indicated on the map by the red region. Therefore it will be sufficient enough to make use of T_1 relaxation at 1.0T for the magnetization at a sample length between 0.5E-9 and 1.0E-9m for the liver.

For the fatty tissues in figure 10, there is high magnetization between 1000 and 5.5E+4ampere/meter for 0.5T, for 1.0T it falls between 4.025E+7 and 4.6+E7ampere/meter and for 1.5T it falls between 8181 and 9350ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.5E-9 and 1.5E-9m.

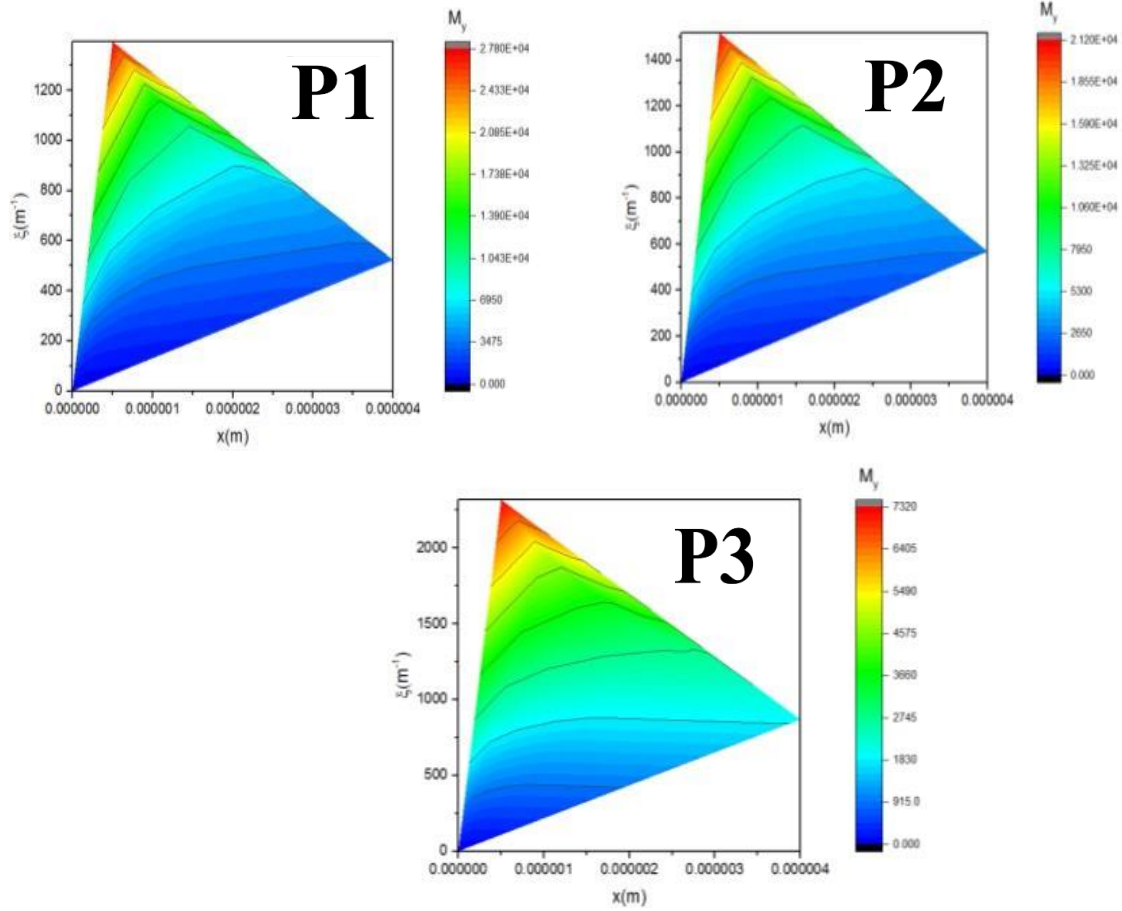


Figure 9. Transverse magnetization map for Liver in the Range of value of x: 0 to 4E-9

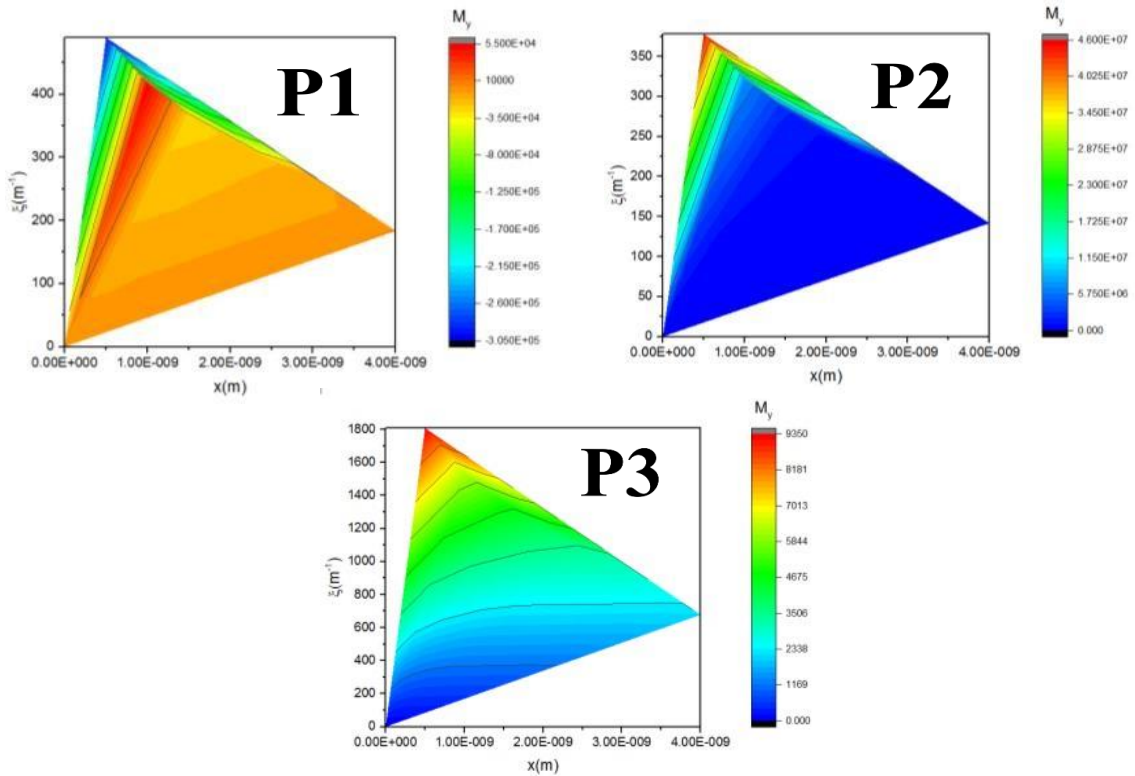


Figure 10. Transverse magnetization fatty tissues in the Range of value of x: 0 to 4E-9

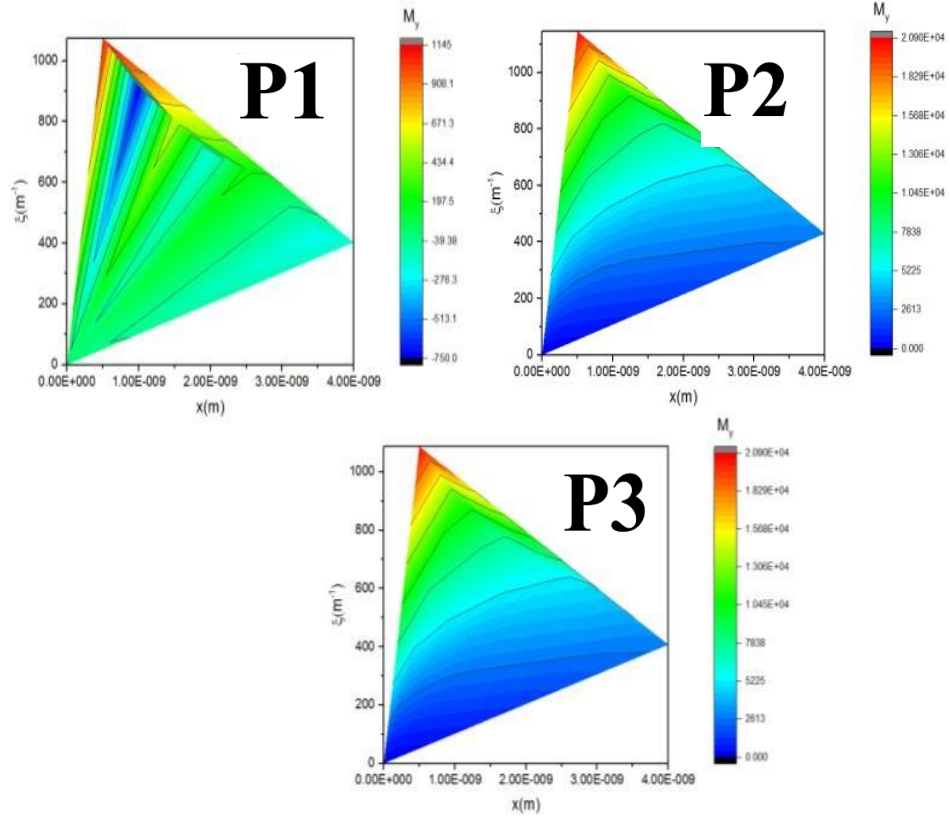


Figure 11. Transverse magnetization map for grey brain matter in Range of value of x: 0 to 4E-9 m

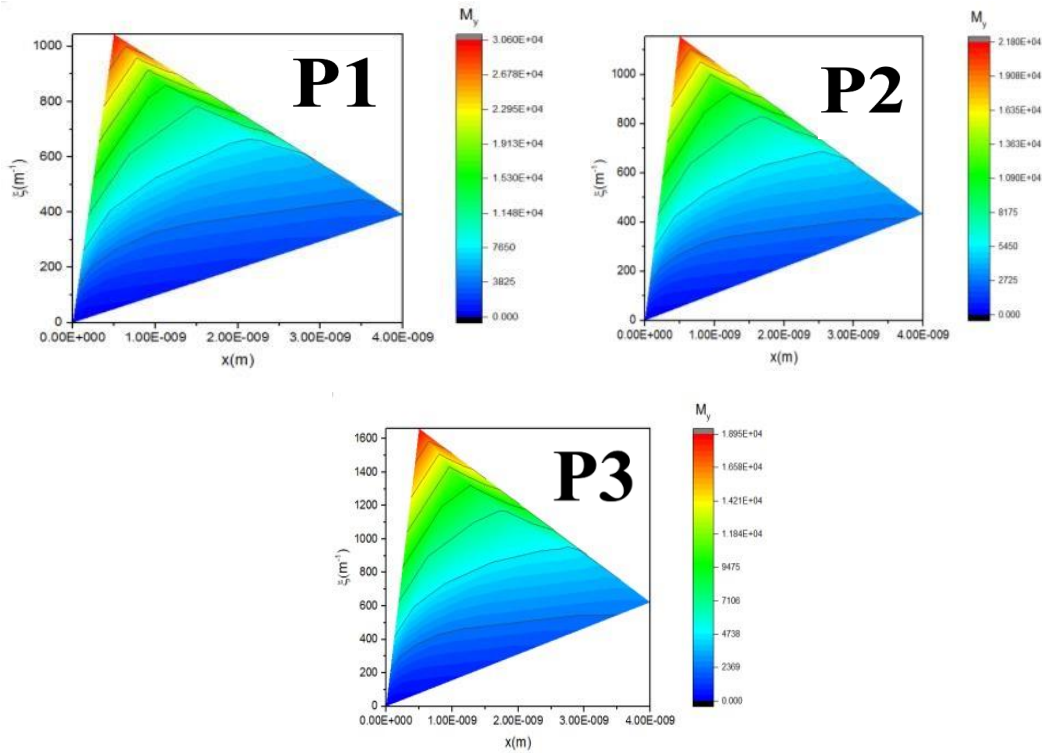


Figure 12. Transverse magnetization map for white brain matter in the Range of value of x: 0 to 4E-9 m

For the grey brain matter shown in figure 11, there is high magnetization between 908.1 and 1145ampere/meter for 0.5T, for 1.0T it falls between 1.82E+4 and 2.090E+4ampere/meter and for 1.5T it falls between 1.892E+4 and 2.090E+4ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.5T for the magnetization at sample length between 0.5E-9 and 1.5E-9m. For the white brain matter (figure 12), there is high magnetization between 2.678E+4 and 3.060E+4ampere/meter for 0.5T, for 1.0T it falls between 1.908E+4 and 2.180E+4ampere/meter and for 1.5T it falls between 1.658E+4 and 1.895E+4ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.0 to 1.5E-9m.

Figure 13 below shows the transverse magnetization maps at sample length between 0 to 4E-9, for the liver, we see that the high magnetization falls in between 5.775E+6 and 6.600E+6ampere/meter for 0.5T, for 1.0T it falls between 3.378E+4 and 3.860E+4ampere/meter and for 1.5T it falls between 4.253E+4 and 4.860E+4ampere/meter. They are indicated on the map by the red region. Therefore, it will be sufficient enough to make use of T_1 relaxation at 1.5T for the magnetization at a sample length between 0E-12 and 1.5E-12m for the liver

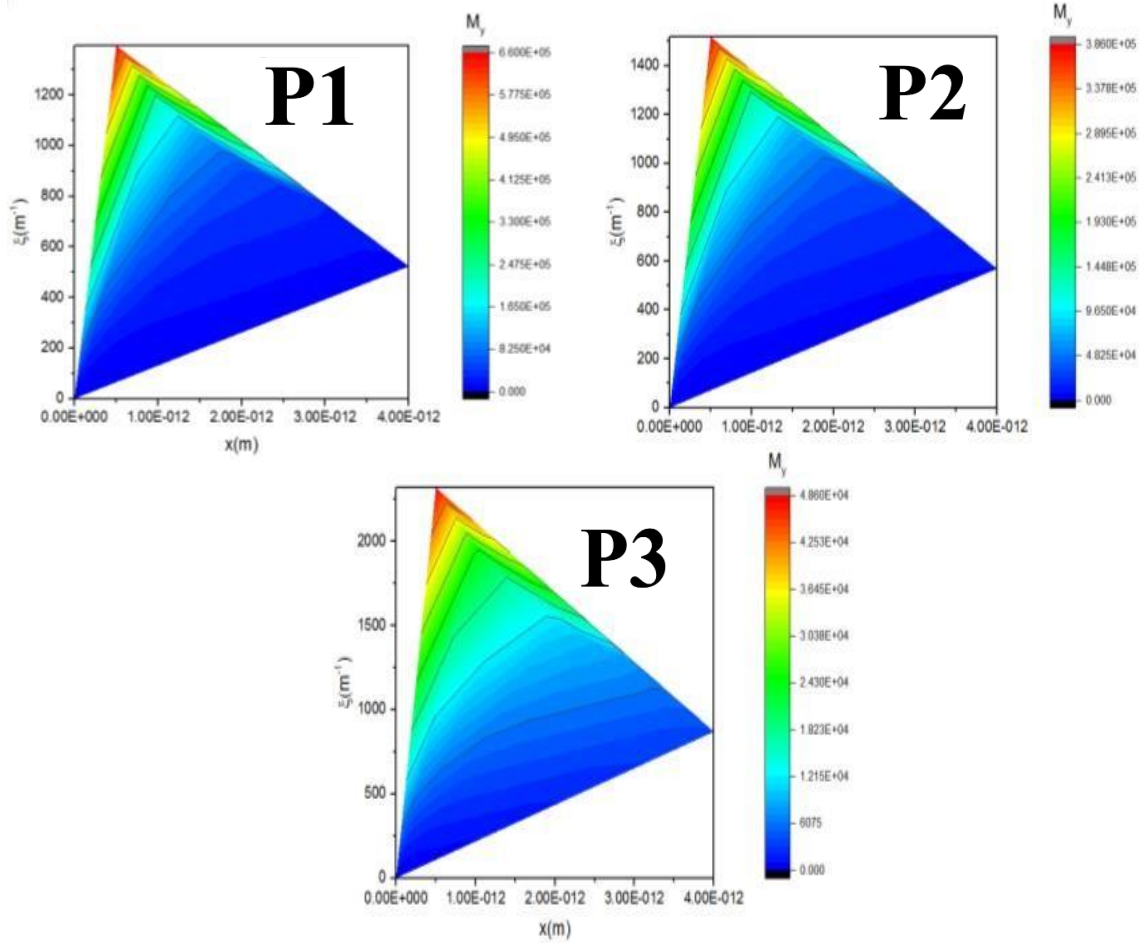


Figure 13. Transverse magnetization map for Liver in the Range of value of x: 0 to 4E-12 m

For the fatty tissues shown in figure 14, there is high magnetization between 7.5E+4 and 5.4E+5ampere/meter for 0.5T, for 1.0T it falls between 1.278E+9 and 1.460E+9ampere/meter and for 1.5T it falls between 1.676E+4 and 1.915E+4 ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T for the magnetization at sample length between 0.0E-12 and 1.0E-12m. For the grey brain matter (figure 15), there is high magnetization between 2493 and 3100ampere/meter for 0.5T, for 1.0T it falls between 4.865E+4 and 5.6560E+4 ampere/meter and for 1.5T it falls between 4.865E+4 and 5.560E+4ampere/meter. They are indicated on the map by the red region. It will be best to make use of 1.0T and 1.5T for the magnetization at sample length between 0.0E12 and 1.0E-12m.

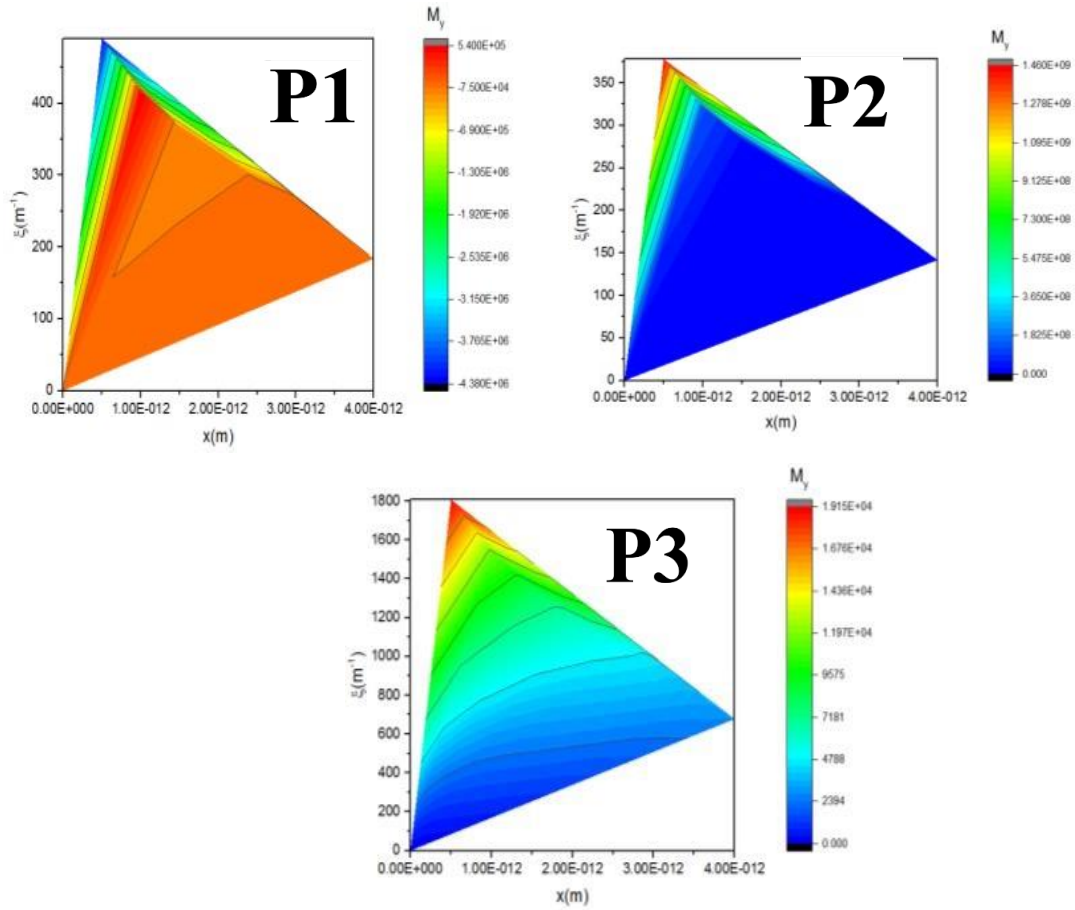


Figure 14. Transverse magnetization map for Fatty tissues in the Range of value of x: 0 to 4E-12 m

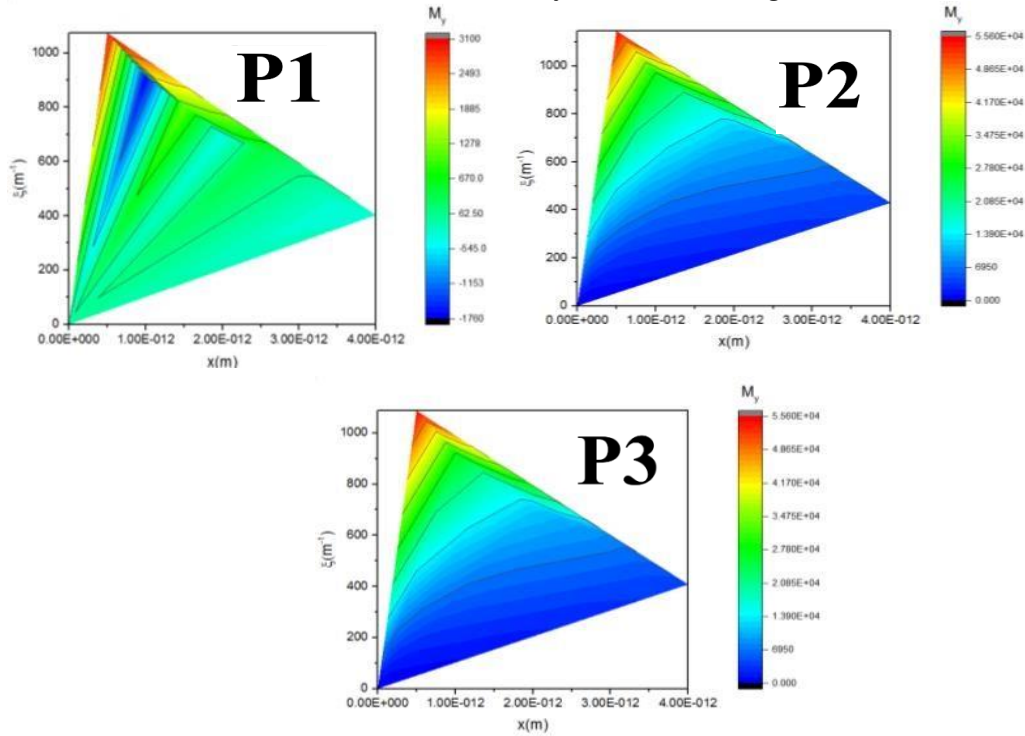


Figure 15. Transverse magnetization map for grey brain matter in the Range of value of x: 0 to 4E-12 m

For the white brain matter shown in figure 16, there is high magnetization between 8.094×10^4 and 9.259×10^4 ampere/meter for 0.5T, for 1.0T it falls between 5.163×10^4 and 5.90×10^4 ampere/meter and for 1.5T it falls between 4.865×10^4 and 5.560×10^4 ampere/meter. They are indicated on the map by the red region. It will be best to make use of 0.5T for the magnetization at sample length between 0.0 to 1.0×10^{-12} m.

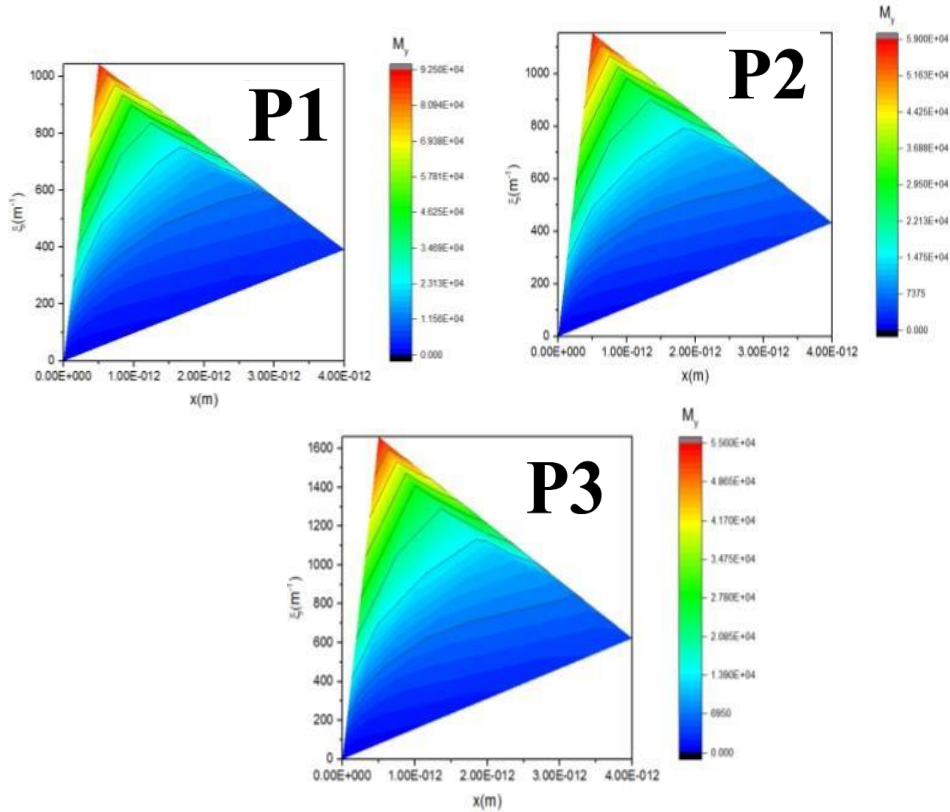


Figure 16. Transverse magnetization map for White brain matter in the Range of value of x: 0 to 4×10^{-12} m

Conclusion

The transverse magnetization maps for the various biological tissues have been obtained with Originpro. We were able to obtain the transverse magnetization, which we made use of to achieved the contour plot. The transverse magnetization plot was done for T_1 relaxation time at 0.5T, 1.0T and 1.5T. Also we obtained the transverse magnetization equation from the Bloch NMR flow equation. The result shows that transverse magnetization was greater at 0.5 T for the tissues considered at the range of 4.5×10^{-12} to 4.5×10^{-5} m. This research work was performed for T_1 relaxation time at 0.5T, 1.0T, and 1.5T. More work should be done to be able to achieve transverse magnetization for T_1 greater than 1.5T and T_1 less than 0.5T. In this research the transverse magnetization was done for contour map plot, I recommend that a 3-D plot should be plot for the transverse magnetization.

Scientific Ethics Declaration

The authors declare that the scientific ethical and legal responsibility of this article published in EPSTEM journal belongs to the authors.

Acknowledgements or Notes

* This article was presented as an oral presentation at the International Conference on Basic Sciences and Technology (www.icbast.net) held in Antalya/Turkey on November 16-19, 2023.

References

- Albrecht, R., Sebag, D., & Verrecchia, E. (2015). Organic matter decomposition: bridging the gap between rock–eval pyrolysis and chemical characterization (CPMAS ^{13}C NMR). *Biogeochemistry*, 122(1), 101-111.
- Awojoyogbe, O. B., Dada, O. M., Faromika, O. P., & Dada, O. E. (2011). Mathematical concept of the Bloch flow equations for general magnetic resonance imaging: A review. *Concepts in Magnetic Resonance Part A*, 38(3), 85-101.
- Becker, E. D. (1993). A brief history of nuclear magnetic resonance. *Analytical chemistry*, 65(6), 295-302.
- Cooley, C. Z., Stockmann, J. P., Armstrong, B. D., Saracanie, M., Lev, M. H., Rosen, M. S., & Wald, L. L. (2015). Two-dimensional imaging in a lightweight portable MRI scanner without gradient coils. *Magnetic Resonance in Medicine*, 73(2), 872-883.
- Farrukh, M. A. (Ed.). (2012). *Advanced aspects of spectroscopy*. BoD–Books on Demand.
- Ginsberg, N. S., Cheng, Y. C., & Fleming, G. R. (2009). Two-dimensional electronic spectroscopy of molecular aggregates. *Accounts of Chemical Research*, 42(9), 1352-1363.
- Giza, S. A., Sethi, S., Smith, L. M., Empey, M. E. E., Morris, L. E., & McKenzie, C. A. (2021). The application of in utero magnetic resonance imaging in the study of the metabolic and cardiovascular consequences of the developmental origins of health and disease. *Journal of Developmental Origins of Health and Disease*, 12(2), 193-202.
- Grover, V. P., Tognarelli, J. M., Crossey, M. M., Cox, I. J., Taylor-Robinson, S. D., & McPhail, M. J. (2015). Magnetic resonance imaging: principles and techniques: lessons for clinicians. *Journal of Clinical and Experimental Hepatology*, 5(3), 246-255.
- Levitt, M. H. (2013). *Spin dynamics: basics of nuclear magnetic resonance*. John Wiley & Sons.
- Lovchinsky, I., Sushkov, A. O., Urbach, E., de Leon, N. P., Choi, S., De Greve, K., & Lukin, M. D. (2016). Nuclear magnetic resonance detection and spectroscopy of single proteins using quantum logic. *Science*, 351(6275), 836-841.
- Mammarappallil, J. G., Rankine, L., Chan, H. F., Weatherley, N., Wild, J., & Driehuys, B. (2019). New developments in imaging idiopathic pulmonary fibrosis with hyperpolarized Xenon MRI. *Journal of Thoracic Imaging*, 34(2), 136.
- Miller, J. F., Harding, S. L., & Tufte, G. (2014). Evolution-in-materio: evolving computation in materials. *Evolutionary Intelligence*, 7(1), 49-67.
- Moser, E., Laistler, E., Schmitt, F., & Kontaxis, G. (2017). Ultra-high field NMR and MRI- the role of magnet technology to increase sensitivity and specificity. *Frontiers in Physics*, 5, 33.
- Nagy, C., & Einwallner, E. (2018). Study of in vivo glucose metabolism in high-fat diet-fed mice using oral glucose tolerance test (OGTT) and insulin tolerance test (ITT). *Journal of Visualized Experiments*, (131).
- Reid, A., Smith, F. W., & Hutchison, J. M. (1982). Nuclear magnetic resonance imaging and its safety implications: follow-up of 181 patients. *The British Journal of Radiology*, 55(658), 784-786.
- Seabolt, L. A., Welch, E. B., & Silver, H. J. (2015). Imaging methods for analyzing body composition in human obesity and cardiometabolic disease. *Annals of the New York Academy of Sciences*, 1353(1), 41-59.

Author Information

Bilyaminu Usman

Zamfara State College of Education
Maru, Nigeria

Contact e-mail: bilyaminumar2@gmail.com

Ahmed Jimoh

Kebbi State University of Science and Technology,
Aliero, Nigeria

To cite this article:

Usman, B. & Jimoh, A. (2023). Numerical computation of NMR magnetization for various tissues in the human body using oringinpro. *The Eurasia Proceedings of Science, Technology, Engineering & Mathematics (EPSTEM)*, 25, 134-149.